

Review

# Magnetic Nanoparticles Used in Oncology

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**Abstract:** Recently, magnetic nanoparticles (MNPs) have more and more often been used in experimental studies on cancer treatments, which have become one of the biggest challenges in medical research. The main goal of this research is to treat and to cure advanced or metastatic cancer with minimal side effects through nanotechnology. Drug delivery approaches take into account the fact that MNPs can be bonded to chemotherapeutic drugs, nucleic acids, synthesized antibodies or radionuclide substances. MNPs can be guided, and different treatment therapies can be applied, under the influence of an external magnetic field. This paper reviews the main MNPs' synthesis methods, functionalization with different materials and highlight the applications in cancer therapy. In this review, we describe cancer cell monitorization based on different types of magnetic nanoparticles, chemotherapy, immunotherapy, magnetic hyperthermia, gene therapy and ferroptosis. Examples of applied treatments on murine models or humans are analyzed, and glioblastoma cancer therapy is detailed in the review. MNPs have an important contribution to diagnostics, investigation, and therapy in the so called theranostics domain. The main conclusion of this paper is that MNPs are very useful in different cancer therapies, with limited side effects, and they can increase the life expectancy of patients with cancer drug resistance.

**Keywords:** magnetic nanoparticles; cancer therapy; drug delivery; radiosensitizing properties; glioblastoma; magnetic hyperthermia; ferroptosis



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## 1. Introduction

Magnetic nanoparticles (MNPs) have been used in nanomedicine and the manufacturing of nanosensors for a long time. It is well known that MNPs have a controlled interaction with an external magnetic field, generated by using permanent magnets; therefore, as a consequence, the position of an MNP could be used to exactly establish where a medical problem exists. An alternating magnetic field induces a thermal heating process in the MNPs, and they are very useful as a contrast substance in nuclear magnetic resonance imaging (MRI) and as drug delivery vehicle for different diseases. The alloys of FeCo, magnetite (Fe<sub>3</sub>O<sub>4</sub>) and maghemite (γ-Fe<sub>2</sub>O<sub>3</sub>) are the most used materials, because a high value of the spin magnetic moment is present [1]. In the case of Fe<sub>3</sub>O<sub>4</sub> the iron and the oxygen atoms are arranged in an inversed spinel structure, and the γ-Fe<sub>2</sub>O<sub>3</sub> is characterized by the fact that the iron is bivalent. The bivalent iron could catalyze the oxidation of the hydrogen peroxide, resulting in toxicity due to the reactive species of oxygen. Usually, maghemite particles must have an outer shell, made with biocompatible materials such as gold or other polymers or resins, to prevent the toxicity of this alloy [2,3].

This paper focuses on magnetic nanoparticles used in oncology, and it provides a comprehensive review on this topic, taking into account specific aspects of the neoplasm treatment. The preparation methods of the MNPs used in medicine, classified as chemical, physical, and biological technologies, are presented.

Magnetic nanoparticles' functionalization is a very important topic, and it will also be taken into account in the discussion. The synthesis process of the MNPs with gold (Au@MNPs) implies two important steps: the synthesis of the iron oxide and the application of a gold shell. The gold shell can be directly applied onto the magnetic core [4–7] or indirectly, by adding a glue-like material layer between the iron oxide and gold shell [8]. Other inorganic and organic compounds such as silica, silver and polymers are also a viable candidate for MNP functionalization [9]. Today, superparamagnetic nanoparticles of iron oxide with a biocompatible shell (SPIONs) are being used more and more often in personalized medicine for the diagnosis and treatment of different types of cancers [2,10–13]. With the help of SPIONs, a real-time monitorization of the treatment is possible, by combining SPIONs with different medicines and then by following the changes that appear in the T1 or T2 relaxivity parameters [14]. The multifunctional SPIONs are a very important factor in immunotherapy, because through SPIONs the modulation of the macrophage polarization is possible, and in the case of a human monocyte cellular line, they can be transformed from the M<sub>2</sub> state (pro-tumorigenic) to the M<sub>1</sub> state (anti-tumorigenic). As an intermediate effect, antigen transport through lymph nodes is possible and activates the dendritic cells that can cause, as a final result, an important response from the T cells [15].

In the case of “in vivo” application, the hydrodynamic dimension of magnetic nanoparticles becomes one of the most important parameters, being restricted by the anatomical characteristics of the human body and by the fact that this type of materials is delivered in an aqueous solution. Nanoparticles smaller than 150 nm could pass the endothelial barrier, but the blood–brain barrier is permeable for magnetic nanoparticles with reduced dimensions and electric neutral lipidic molecules with a concentration lower than 500 g/mol [16–18]. The area to volume ratio is a limitative factor, which is taken into consideration in the nanoparticle synthesis process.

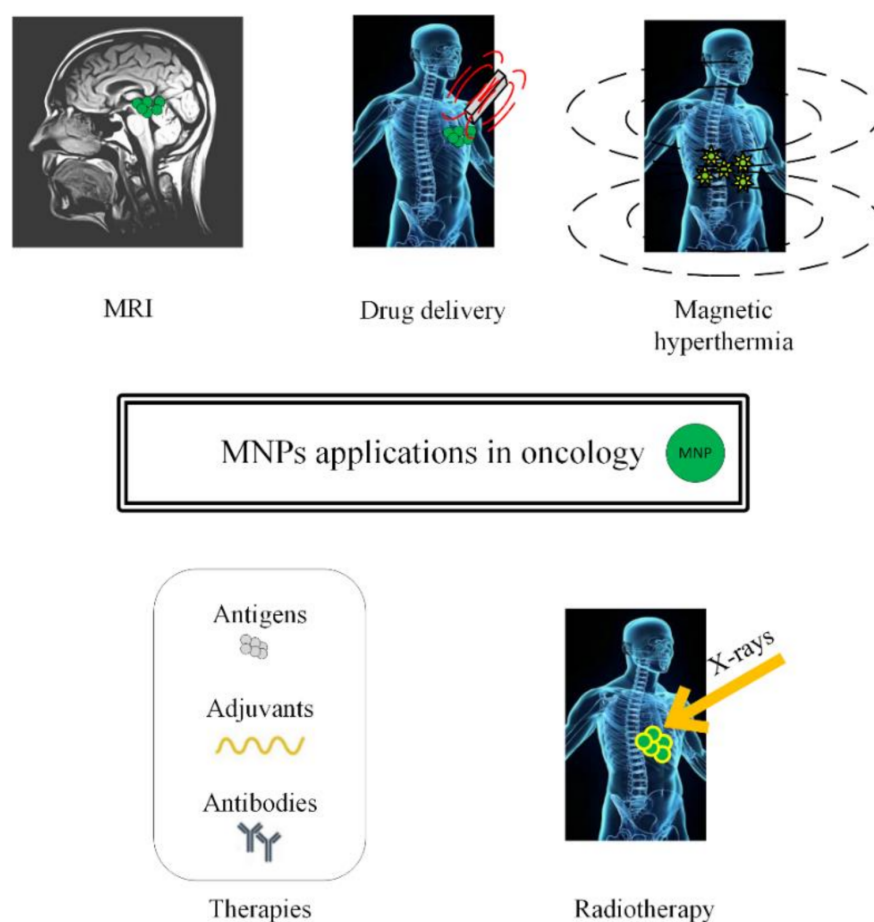
Magnetic nanoparticles tend to form aggregates that are very important if the material is used as a contrast substance in magnetic resonance investigations [19–21]. MNPs also possess numerous advantages, such as a large surface area to volume ratio, pore sizes, functionalized surfaces, multiple sites for interaction or binding, and low mass transfer resistance, which makes them very suitable to be used in different disease treatments.

In this review, we will present different approaches to treat cancer by combining chemotherapy, radiotherapy, immunotherapy, and gene therapy with MNPs or SPIONs, as depicted in Figure 1.

Magnetic-induced hyperthermia uses SPIONs to destroy the malignant tissues, which are difficult to treat through conventional therapies, and it will be detailed in Section 5. The tumoral tissues are targeted with SPIONs, whose magnetic properties are enhanced by using an external alternating magnetic field that induces a heating process in the neoplasm area. It is well known that by increasing the tissue temperature above 42 °C, the structural and functional proteins alter and the necrosis of the tumoral tissue begins.

The ferroptosis process will also be discussed and the side effects of the MNPs or SPIONs treatment will be highlighted in the final section of this review. The challenges of these innovative treatments will be presented.

Today, these treatments are successfully applied in murine animal models, but these approaches are considered very useful in the case of cerebral cancers such as glioblastoma, and they could be lifesaving in patient cases, where classical treatments provide poor results.



**Figure 1.** Schematic representation of magnetic nanoparticles' applications in oncology (MRI investigations, drug delivery in chemotherapy, magnetic hyperthermia, immunotherapy and radiotherapy).

## 2. Magnetic Nanoparticles' Synthesis

In the case of biomedical applications, there are some important restrictions, which must be taken into account. Each medical investigation and treatment requires special and dedicated nanoparticles. The surface effects, the crystallinity grade, and the link between the magnetic properties and the dimensions or shapes of the nanoparticles should be considered. Currently, the ideal shape of a magnetic nanoparticle is spherical or quasi-spherical.

The synthesis process can be divided into three principal categories as a function of the aggregation state of the precursors (gaseous, aqueous, or solid). Another classification can be performed as a function of the process type (chemical, physical, or biological). The most important synthesis methods presented in the literature are co-precipitation, sol-gel procedure, and hydrothermal synthesis [22]. Additionally, new methods were developed, such as microemulsion, thermal decomposition, sonolysis, and biosynthesis [23]. In Table 1, the main synthesis procedures that are used in practice are presented.

One of the most commonly used chemical methods is co-precipitation. The synthesis process of the nanoparticles used in this method can be completed in an open or closed environment. The open medium includes the following steps: co-precipitation, hot organic solvent use, a gaseous route or solid chemical reactions, and the closed medium involves oil- or water-based microemulsions and porous inorganic or organic templates. In Figure 2 are presented scanning electron microscopy (SEM) images of MNPs obtained through the co-precipitation method at different magnification scales.

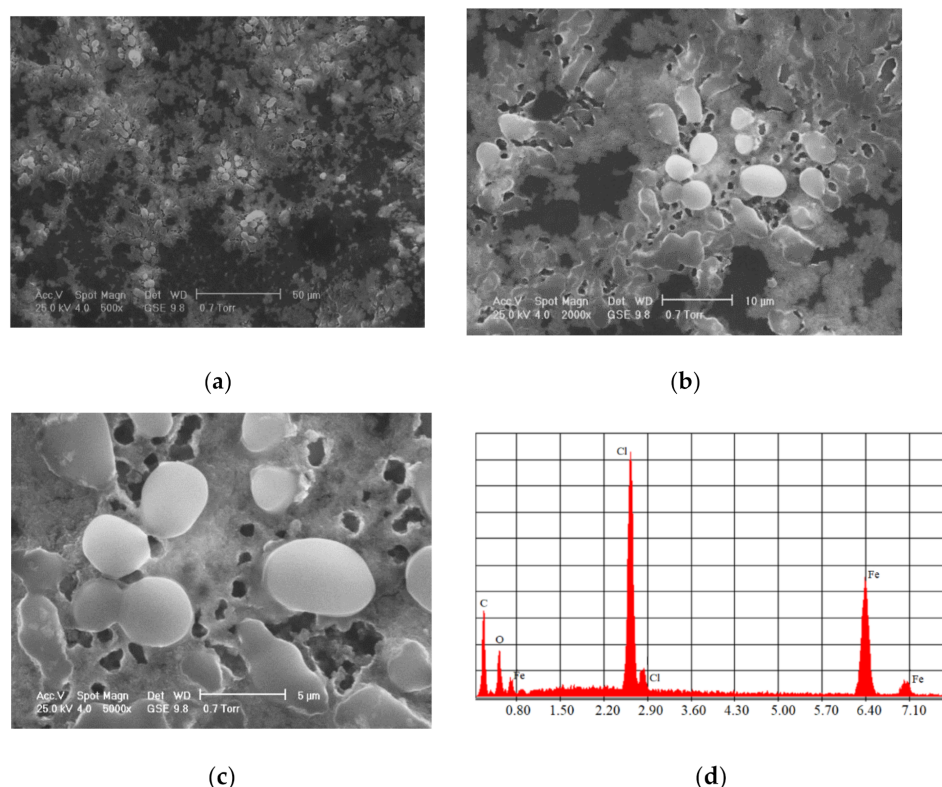
**Table 1.** Synthesis methods for magnetic nanoparticles.

	Synthesis Method	Conditions	Size (nm)	Particle Morphology	Reference
Chemical methods	Aqueous co-precipitation	Temperature 20–90 °C Water solvent	15–200	Spherical, rhombic	[24]
	Sol-gel synthesis	Temperature 200–400 °C Organic solvent	20–200	Spherical	[23]
	Hydrothermal synthesis	Temperature 220 °C Water-ethanol solvent	520	Spherical	[25]
	Microemulsions	Temperature 20–50 °C Organic solvent	4–12	Spherical, cubic	[26]
	Electrochemical deposition	Temperature 70–100 °C Organic solvent	3–8	Spherical	[22]
	Polyol method	Temperature 120–280 °C Organic solvent	5–40	Spherical	[22]
Physical methods	Sonochemical method	Temperature 25 °C Water	10–30	Spherical, rod	[22]
	Thermal decomposition	Temperature 100–320 °C Organic	3–20	Spherical	[25]
	Spray pyrolysis	Temperature 400–700 °C Organic	5–60	Spherical with aggregates	[27]
	Laser-induced pyrolysis	Temperature 1100 °C Organic	5–30	Spherical less large	[27]
Biological methods	Biomimetic synthesis	-	50–100	Spherical cluster, Cubo-octahedral	[28]
	Microbial synthesis	Virus Tobacco mosaic virus	5	Disordered, prismatic and film	[28,29]
	Plant-mediated synthesis	Eucalyptus Leaf	20–80	Spheroidal	[28]

The co-precipitation in an aqueous solution consists of using Fe<sup>2+</sup> and Fe<sup>3+</sup> precursors, dissolved in an aqueous solution and then mixed with reactive substances, in order to precipitate in the spinel system. In the case of the Massart method [30], a degassed solution of chlorides based on Fe<sup>2+</sup> and Fe<sup>3+</sup> is added to an ammonia solution, washed several times, and then stabilized in basic or acid suspensions. The aqueous medium is kept at a low temperature, and thus the co-precipitation method is considered to be one of the most commonly used technologies [31,32].

Other methods are based on hot organic solvents instead of water. When the dimensions of the particles are between 15 and 20 nm, through the co-precipitation method, using a Fe<sub>2</sub>SO<sub>4</sub> precursor combined with a weak oxidant, high-quality nanoparticles are obtained [33–37].

In the case of hot organic solvents, MNPs with a high grade of crystallinity and a good monodispersing property are synthesized. The main mechanisms are nucleation and growth, and the coordination ligands are used to impose a good dispersion grade of the magnetic nanoparticles, which have a passivate surface. The particle dimension depends on the boiling temperature of the solvent. This technology consists of mixing the substances at room temperature; then an increase in the temperature is supposed to be applied at a value at which magnetic nanoparticles are rapidly formed. These particles have hydrophobic properties, and they are transferred to an aqueous medium and used in biomedical applications. Some FePt or FePt-Au magnetic nanoparticles are obtained based on crystalline iron oxide, formed from an iron precursor such as Fe(acac)<sub>3</sub>, lauric acid or lauryl ammine [37].



**Figure 2.** SEM analysis made in the case of Fe<sub>3</sub>O<sub>4</sub> MNPs obtained through the co-precipitation method at three different magnification scales: (a) 500×; (b) 200×; (c) 5000×; and the resulting elemental analysis (d).

Another important method is the growth of magnetic nanoparticles in limitative conditions (growth under confinement) and the dimensions and shape of the nanoparticles are controlled [38,39]. This closed domain could be considered a matrix that represents a barrier used to control the material nucleus growth. This matrix could be beneficial for obtaining special properties of the magnetic material. Organized surfactants such as microemulsions, defined as thermodynamic stable dispersions, and composed of two non-miscible liquids, are usually employed. The surfactant determines microcavity formation, which represents the closure area. In this way, nucleation, growth and particle agglomeration are avoided. A classical case is the Al<sub>2</sub>O<sub>3</sub> matrix with cylindrical pores [40].

The sol-gel process is based on the hydrolysis and condensation chemical reactions of metal precursors at low temperatures, resulting in the formation of an inorganic network [41]. The conversion of monomers into a colloidal solution determines the sol, and the gel is produced after the evaporation of the solvent, and by introducing particles in the inorganic network. Through this method, single-phase, fine, dense, and homogenous MNPs can be obtained. Although the sol-gel process is environmentally friendly and it is not an expensive method, it presents with a limited efficiency, and the synthesis process is longer than in the case of the co-precipitation method.

The hydrothermal method consists of MNPs' generation through a mixture between aqueous bivalent metals in acetate solutions with iron nitrate and a carbon nano template at a pH higher than 7. The final product is washed, centrifuged and annealed at 500 °C, in order to eliminate the carbon compounds. Ethylenediamine or citric acid can be used in the synthesis process [42].

Another important method is based on polyol. The metal ions are reduced in a polyol solution and precipitate as nanoparticles with dimensions lower than 100 nm. [43]. MNPs with small sizes can be obtained on dendrimer platforms or by using ultrasound waves [44]. Electrochemical deposition of metal is used to synthesize MNPs, by reducing the metallic ions dissolved by anode and by depositing them at the cathode. Pyrolysis, Fe<sup>3+</sup> spray

solution or the CO<sub>2</sub> laser heating process of gases that contain iron precursors were also reported as synthesis methods for MNPs [43].

The biological synthesis technologies are based on plants (bark, leaf, root, fruit, seed, flower), fungus, bacteria, algae, virus, and marine organisms, and they are considered simple, low-cost, non-toxic and eco-friendly. Two examples, applied in the case of iron-based MNPs, are presented in Table 1.

Another preparation method consists of metal–organic material structures, inside which the metallic ions are combined with organic molecules. The inorganic matrices have superior chemical and mechanical properties. The most used inorganic matrix is that based on silica, but carbon nanotubes or materials with a structure similar to graphene or titania nanotubes are also seen in practice. The magnetic nanoparticles are encapsulated in silica, by using ammonia hydroxide through the Stoeber method [45]. Carbon nanotubes were treated with nitric acid in an FeCl<sub>3</sub> suspension [46].

The gaseous state synthesis is very suitable for the manufacture of magnetic nanoparticles with dimensions lower than 5 nm. This method is based on the formation of gaseous substances oversaturated with vapors due to chemical reactions. The oversaturated vapor state contains atoms or molecules of a material, set at a higher pressure than vapor pressure. New particles are nucleated through laser pyrolysis or using carbonyl precursors. The pyrolysis is performed using the heating process of a gaseous mixed compound with the help of a continuous laser wave, which initiates and maintains the decomposition reaction. Once an energy level is reached, the metal atoms are produced through a fast coalescence procedure, resulting in nanoparticles which can supplementarily react with another gas components [47,48].

Through solid synthesis, MNPs with sizes lower than 20 nm can be obtained, but this method is rarely used.

The chemical and physical methods are considered conventional technologies and they are characterized by high costs and complex procedures. Co-precipitation and thermal/hydrothermal decomposition are the most commonly used methods because they are easy and secure.

### 3. Functionalization of Magnetic Nanoparticles

The encapsulation and coating of magnetic nanoparticles represent two important steps, which could be adopted in the MNPs synthesis for medical applications. Usually, hydrophilic substances are used, which are suitable for blood circulation and protein adhesion. Sometimes, thin polymers can be utilized [49,50]. If an organic matrix is involved, the human body does not present an immune response. Synthetic or natural polymer matrices made from polysaccharides or polyesters using the co-precipitation method are also a suitable solution.

The type of the coating which is applied on an MNP is important, because the shell layer could enhance or reduce the magnetic properties of the core, the shell thickness, and the size of the nanoparticles. The main methods used for MNPs' functionalization are performed in situ or post synthesis, involving mechanisms such as ligand addition, ligand exchange or encapsulation.

#### 3.1. Inorganic Compounds

In the case of inorganic compounds, a specific group of ligands should be chosen, in order to manifest a high affinity for MNPs. The inorganic materials used in functionalization process are gold, silica, or silver.

Gold is an inert metal, and it is resistive to oxidation and corrosion. Nowadays, there are a high number of techniques associated with gold deposition, such as sputtering, thermal evaporation, and chemical deposition.

Magnetic nanoparticles for medical applications, functionalized with gold, can be considered as a magnetic core covered with a gold shell (Fe<sub>3</sub>O<sub>4</sub>@Au).

The synthesis procedure of  $\text{Fe}_3\text{O}_4@Au$  nanoparticles includes two steps: firstly, the iron oxide synthesis and secondly the gold shell application. There are two principal methods used to obtain a gold shell, as shown in Figure 3. The first one is called the direct method, where the gold shell is directly formed on the magnetic material; in the second case—the indirect method—a glue-like intermediary material is used [51].

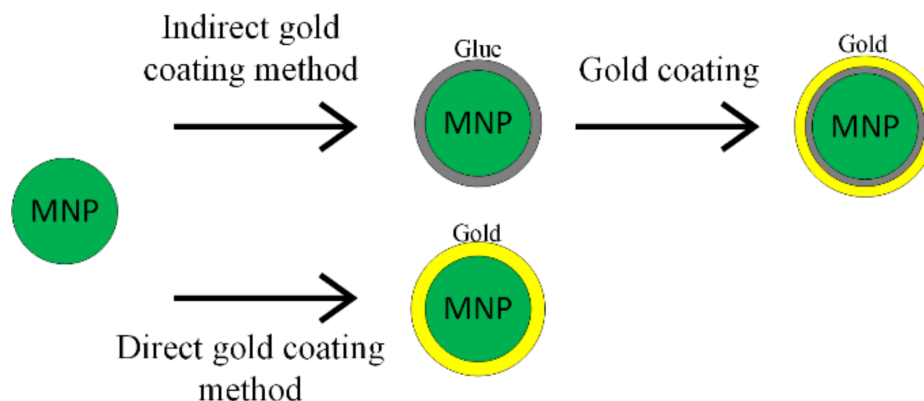


Figure 3. Gold coating methods' schematic representation.

The gold shell can be applied when the magnetite particles are placed in an aqueous solution or in an inorganic material. For the aqueous solution case, the gold shell is created by reducing the  $\text{Au}^{3+}$  ions through ammonium citrate or borohydride [52]. A disadvantage of this method consists of the fact that if the experimental conditions are not entirely respected and controlled, individual gold nanoparticles appear, and outer gold shell formation becomes impossible. When the magnetic core is included in an organic phase such as oleic acid, the gold outer shell can be formed [53]. The synthesis of  $Au@MNPs$  is possible when a non-polar solvent is present, and the obtained gold shell is thick.

Another method in gold functionalization is inverse micelle technology, which is a complicated procedure in which cetyltrimethylammonium bromide, octan and 1-butan are used as surfactants and oil is used as a co-surfactant [52].

The gold shell can also be obtained through the indirect method, interposing a glue layer between the magnetic core and the gold outer shell, as presented in Figure 4 [52,53]. The gold shell must completely cover the magnetic core, in order to ensure a high chemical and physical stability. It has to contain a large number of chemical groups, such as poly-L-histidina, cross-linked polymer (cyclotriphosphazene-co-4, 4'-sulfonyldiphenol) (PZS), polyethylene-imine or silica that can chelate with metallic ions.

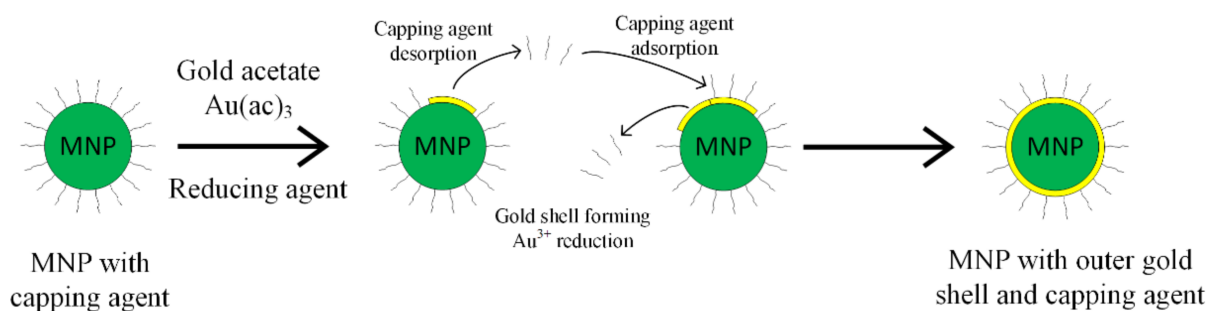


Figure 4. Capping agent desorption and gold coating principle.

When the gold shell was formed on a substrate as silica, the co-precipitation method was applied to synthesize the magnetic core and then sol-gel technology, based on the hydrolysis process of tetraethyl ortho-silicate, was used to obtain the silica cover. Three layers of positive charged poly-electrolytes are formed on the magnetic nanoparticles

covered with silica. The Au ions are negatively charged, and a gold shell can be obtained through the self-assembly method. Gold shells thicker than 30 nm were reported in [54,55].

The functionalization of MNPs with gold presents several advantages in biomedical applications, because it has a positive impact on the specific sensitivity and compatibility. Au@MNPs can form aggregates due to the magnetic attraction forces developed between particles. The surface changes play an important role in the stability increase, which is affected by the electrostatic exchanges on the material's surface. The gold shell prevents the metal ion emission from the magnetic core, increasing the MNPs' biocompatibility [56,57].

*Silver coatings* facilitate the germicidal action of the MNPs, and they are very similar to gold coatings. Silver can generate core-shell structures and heterostructures. Hybrid nanoparticles of Fe<sub>3</sub>O<sub>4</sub>@C@Ag were used for drug release, MRI and two-photon fluorescence imaging, presenting advantages due to having on their surface both carbon and silver.

*Silica* (SiO<sub>2</sub>) is functionalized with MNPs through a similar process to ligand absorption. A silica coating inhibits the aggregation of the MNPs and improves the chemical stability and biocompatibility of the shell-core assembly. Two main methods have been developed to stabilize the silica coating. The first one consists of shielding the magnetic dipole interaction with the silica coating, and the second one is based on charging the MNPs with negative charge, so an electric repulsion phenomenon appears between the shell and the core. SiO<sub>2</sub>@MNPs could be prepared according to the Stober method, in which SiO<sub>2</sub> is generated through hydrolysis and condensation of a sol-gel precursor (tetraethyl orthosilicate, TEOS). As an example, in [58,59], 200 mg of Fe<sub>3</sub>O<sub>4</sub> was introduced in an ethanol suspension under ultrasonic irradiation for 30 min in nitrogen atmosphere. Then, 11 mL of NH<sub>3</sub> (28%) and 400 µL of tetra-ortho-silicate (TEOS) in the Fe<sub>3</sub>O<sub>4</sub> suspension were sonicated for 2 h. The final compound, Fe<sub>3</sub>O<sub>4</sub>@SiO<sub>2</sub>, was washed in ethanol and then collected through a magnetic separation procedure.

The second method is the silica deposition from silicic acid solution, and through this method, the particle size can be effectively controlled. Additionally, a higher percentage of the MNPs' surface can be covered.

The emulsion method consists of controlling the silica shell using micelles or inverse micelles. This procedure is based on the separation of the core-shell MNPs from surfactants linked to the emulsion system.

A main advantage of silica coatings is the presence of surface silanol groups that react with coupling agents, and ligands can be attached to MNPs. In this way, amine groups were introduced on the surface of Fe<sub>3</sub>O<sub>4</sub>@SiO<sub>2</sub> through hydrolysis and condensation of an organosilane (silanization method). Biomolecules could be easily added by using alkoxysilanes with active groups.

Another method for obtaining potential vectors for drug-delivery treatments involving magnetic nanostructures is based on silica mesoporous structured materials (MCMs). Usually, nonmagnetic or magnetic silica nanoparticles are prepared using the sol-gel procedure based on silica xerogels, hydrothermal synthesis and laser pyrolysis. MCMs present a large surface zone and small pores with dimensions between 15 and 100 Å. The pore openings are hexagonal (MCM-14), cubic (MCM-48) and lamellar (MCM-50) ordered. In [60], the drug miltefosine (hexadecyl 2-(trimethylazaniumyl) ethyl phosphate), used for different fungi, bacteria, cancers and parasite species, was loaded onto a new composite mesoporous silica drug carrier 20–30 nm in size, which contains magnetic nanoparticles modified with NH<sub>2</sub> and PEG chains. It was concluded that about 11–25% of the drug content was deposited inside the pores of the silica carrier. Miltefosine loaded onto PEGylated magnetic silica magnetite nanoparticles exhibits a very good antiproliferative activity and antineoplastic potential against human tumor HUT-78 cell line (cutaneous T lymphocytes). This material exhibits important properties as a nanocarrier of miltefosine.

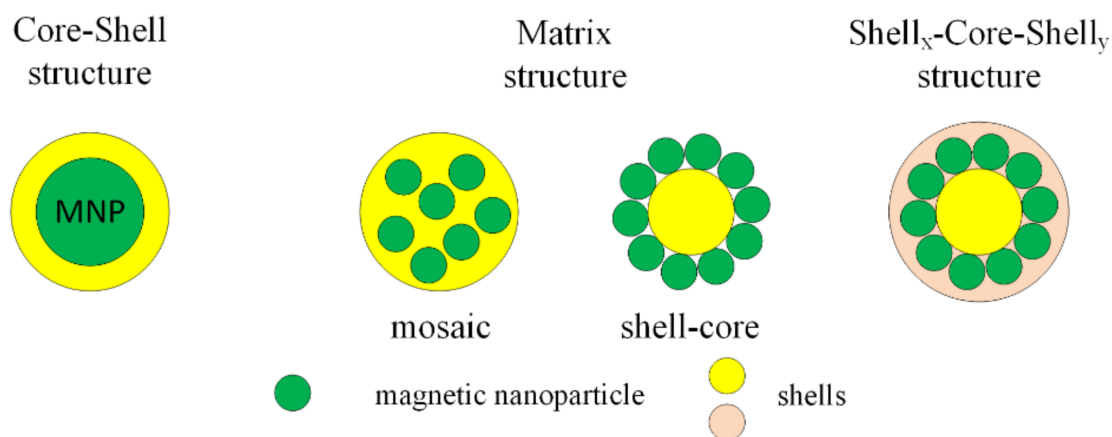
In the nanoscale range, nanoporous silica particles can also be used that can cover the MNPs and embed different oncological drugs on the silica support. A SO<sub>3</sub>H-functionalized magnetic nanoporous silica/polymer nanocomposite was developed in [61]. Spherical



100 nm particles were synthesized that had the anticancer drug mitoxantrone (MTX) loaded in the magnetic nanoporous silica support, covered with a chitosan layer infused with prednisolone (PRD). The final coating layer consisted of alginate. The cytotoxic activity was assessed against HD-MY-Z (Hodgkin lymphoma), EJ (urinary bladder carcinoma) and K-562 (myelogenous leukemia) cellular lines, and this innovative material shows great potential in pharmacological applications.

### 3.2. Organic Compounds

MNPs can be functionalized with organic compounds after or during the synthesis process. Organic functional materials present a good biocompatibility and biodegradability and do not have an important influence on the magnetic properties of MNPs. The functional groups are carboxyl, aldehyde, hydroxyl and amino, which, after the functionalization of MNPs with organic compounds, can be linked to deoxyribonucleic acid (DNA), proteins, enzymes or antibodies. After the functionalization process, the final structure is classified into three types: core-shell, matrix (mosaic or shell-core) and shell<sub>x</sub>-core-shell<sub>y</sub> (Figure 5).

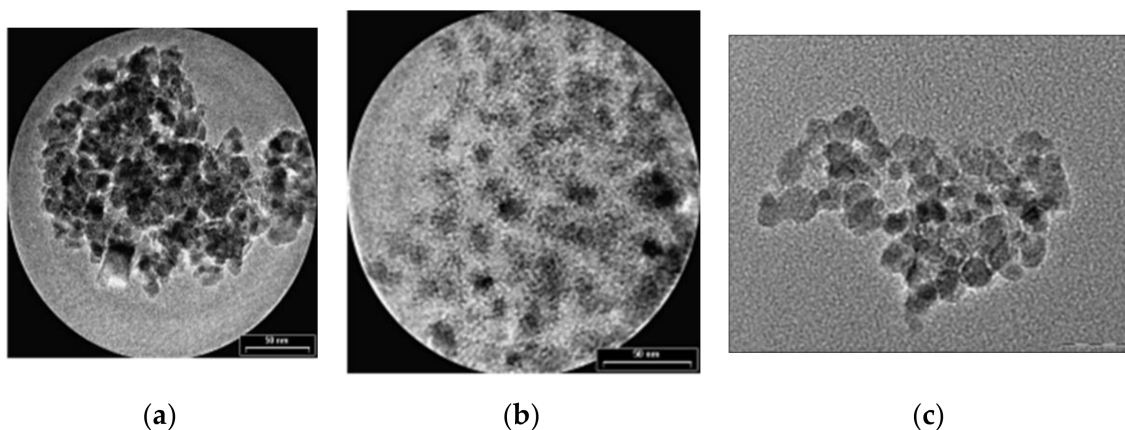


**Figure 5.** Classification of functionalized structure types with organic compound.

The most important organic compounds that can be used in the functionalization of MNPs will be detailed and explain in the review.

The first type of organic compound is the *monomer* class that includes *citrates* and *phosphates*. The surface of MNPs is stabilized in an aqueous solution through the adsorption of citric acid, which have carboxyl groups. The acid is adsorbed on the nanoparticle surface with the help of carboxylate functionalities. This process is dependent on the size and the shape of the particle. MNPs functionalized with citrates are characterized by a negative charge on the particle surface, generating hydrophilic properties. In Figure 6, transmission electron microscopy (TEM) images of Fe<sub>3</sub>O<sub>4</sub> nanoparticles synthesized through the co-precipitation method are presented. It can be observed that the unfunctionalized MNPs tend to form aggregates, since the citrate-functionalized MNPs present a spherical shape and a relatively uniform dispersion.

Regarding the phosphates group, alkanesulfonic and alkanephosphonic acids can be used as surfactants. After the functionalization with phosphates, the dispersions of MNPs are thermodynamically stable. This method was used to prepare SPIONs, based on magnetite, through co-precipitation of bivalent and trivalent iron ions, using poly(vinylalcohol phosphate) (PVAP). The size of the particles is strongly dependent on the PVAP concentration [50]. From Figure 6c, it can be seen that MNPs functionalized with phosphates tend to form aggregates, a fact that makes them very useful in MRI investigations.



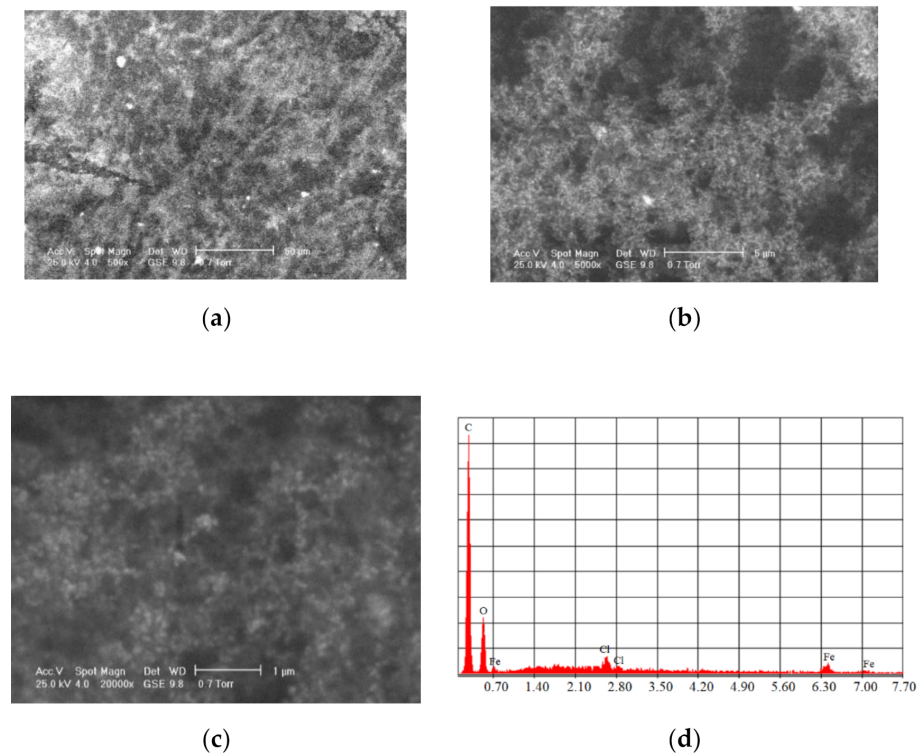
**Figure 6.** TEM images of  $\text{Fe}_3\text{O}_4$  MNPs: (a) unfunctionalized MNPs (average medium size of particles  $8.5 \pm 2$  nm); (b) citrate-functionalized MNPs (average medium size of particles  $9.5 \pm 1$  nm); (c) phosphate-functionalized MNPs.

If *small molecules* are employed in MNP functionalization, they are characterized by a low value of the hydrodynamic radius, a fact that is beneficial for nanotechnology. *Short chain aminosilanes* or *amines* are usually used to coat the MNPs' surface. Magnetite nanoparticles, functionalized with these substances, were considered as being highly water-stable. Another type of small molecule is thiol as an organosulfur compound, 2,3-meso dimercaptosuccinic acid (DMSA), which is characterized through two thiol and two carboxyl groups. It was observed that thiol-functionalized nanoparticles are stable under physiological pH. The stability of the coating could be increased if DMSA is protected through a polyethylene glycol (PEG) chain.

In the *macromolecules* class, natural or synthetic polymers are intensively added for MNPs' functionalization. A polymer coating balances the van der Waals and magnetic attraction forces, which acts on MNPs. Coating approaches, performed in situ and post-synthesis, are based on reaction mixtures that are simultaneously combined with polymer functionalization. Ligand exchange and ligand adsorption are used together to provide a stable structure. In the case of MNPs' functionalization with polymers, the agglomeration of the particles is prevented, and different surface properties are obtained.

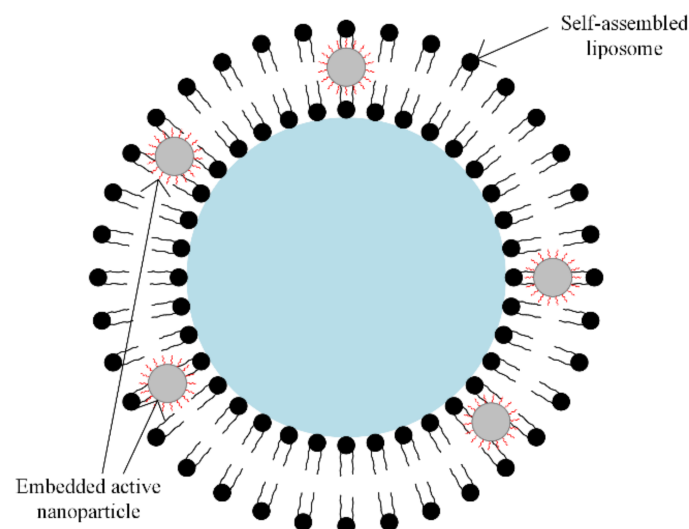
The most commonly used *natural polymers* are *dextran* and *chitosan*. Dextran increases the MNPs' biocompatibility and is a polysaccharide composed of R-D glucopyranosyl. This polymer's presence limits the particle size, and it has the advantage that it can be aminated using ammonia, which permits conjugation with complementary chemical groups. Chitosan is alkaline-based, biodegradable, biocompatible, and hydrophilic. MNPs functionalized with chitosan have shown a high MRI contrast and they exhibit very good properties as carriers in different types of treatments [62]. Figure 7 shows SEM analysis performed for  $\text{Fe}_3\text{O}_4$  functionalized with chitosan.

*Polyethylene glycol* (PEG) is a synthetic, hydrophilic, and biocompatible polymer. PEG-coated magnetite nanoparticles present solubility and stability in physiological and aqueous media. Post-synthesis coating technology is preferred in the case of PEG functionalization. *Polyvinil alcohol* (PVA) is a synthetic polymer that can be transformed into gel, and it is highly biocompatible and hydrophilic. A PVA coating prevents self-agglomeration, and the colloidal stability of the PVA-coated particles is good. *Alginate* is another type of synthetic polymer, and it can be characterized as an electrolytic polysaccharide with carboxyl groups, which interact with iron, resulting in the stable assembly of alginate MNPs due to electrostatic repulsion.



**Figure 7.** SEM analysis made in the case of  $\text{Fe}_3\text{O}_4$  MNPs obtained through the co-precipitation method functionalized with chitosan at different magnification scales: (a) 500 $\times$ ; (b) 5000 $\times$ ; (c) 20,000 $\times$ ; and the resulting elemental analysis (d).

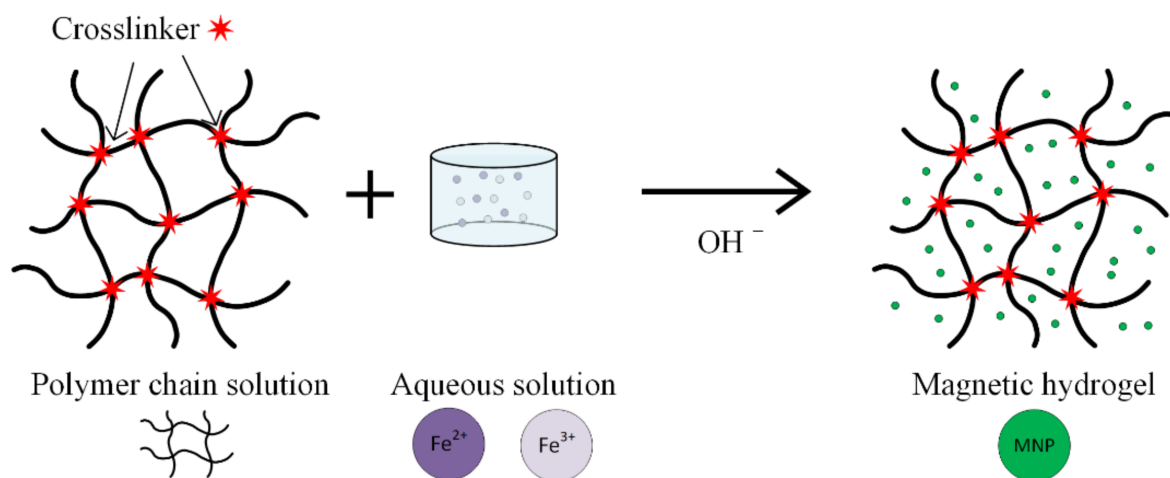
A special class of synthetic polymers is the *liposomes*. In magnetic drug targeting therapy, the liposomes play the role of carriers, because they present a large encapsulation domain, and biomolecules such as DNA or proteins can be encapsulated by liposomes as one unit [63,64]. The liposomes can be combined with different types of magnetic particles, using the dialysis process of a single unilamellar vesicle or through the extrusion of a combination between phospholipids and magnetic particles, as presented in Figure 8.



**Figure 8.** Self-assembled liposome combined with nanoparticles. Solid or water-soluble drugs can be included inside the core region (blue zone) and between interfaces (black spheres); embedded active nanoparticles or oil-soluble drugs in the lipid bilayer can be included.

*Micelles* or *micellar polymers* can be used as a coating layer for MNPs, and they are made from self-assembled amphiphilic polymers, which contain both hydrophobic and hydrophilic groups. The hydrophobic core helps to facilitate the hydrophobic components' movements, and the hydrophilic shell determines the MNP's high stability in the biologic medium [65,66]. The micelles are beneficial for MNP aggregation, in the case of contrast substances used in nuclear magnetic resonance [67].

*Hydrogels* are considered one of the most promising substances, used in magnetic nanoparticle synthesis for medical applications (Figure 9). These are networks of hydrophilic polymers that contain a high amount of water or physiological fluids. The hydrogels exhibit a high biocompatibility and important therapeutical properties [40,68–72]. When nanogels are used, interactions between materials and living cells are possible, and different types of drugs can be delivered.



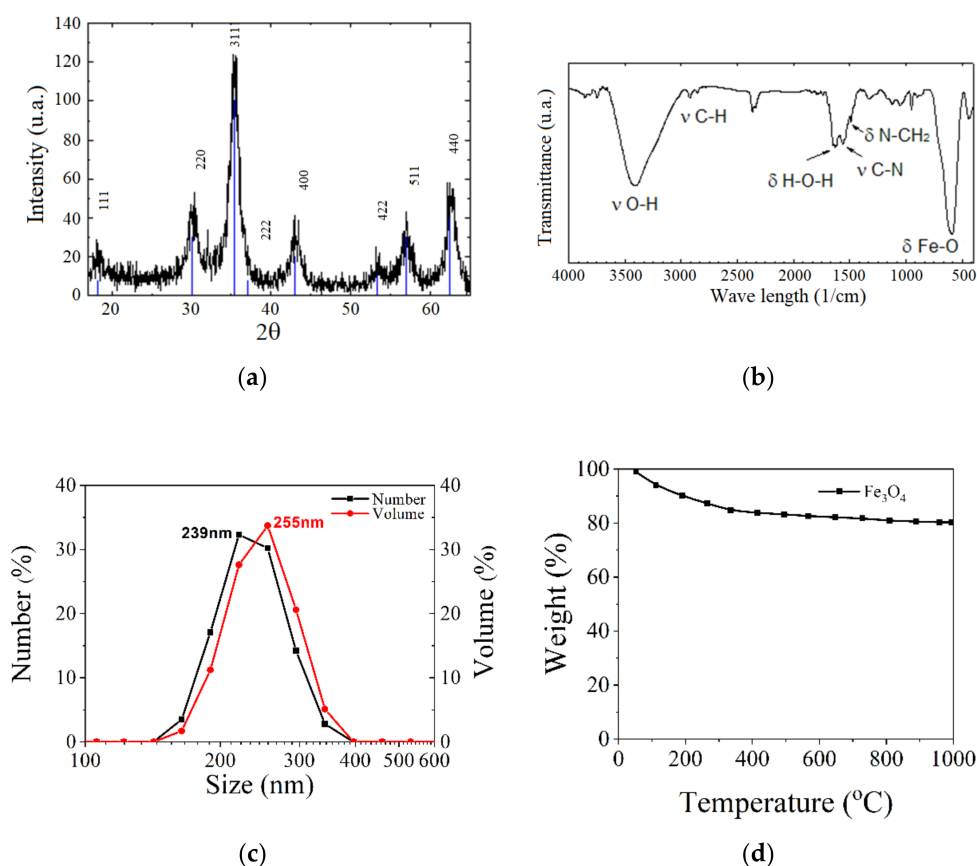
**Figure 9.** Schematic representation of the in situ co-precipitation method used to prepare a magnetic hydrogel.

Polymeric nanogels in aqueous medium are obtained through the co-polymerization of N-vinylcaprolactam or vinylimidazole in aqueous solution in the presence of a link agent and a reaction initiator, soluble in water [70]. The high grade of porosity of these nanogels permits their use as templates for MNPs, through the hydrolysis reaction of FeCl<sub>2</sub> or FeCl<sub>3</sub>.

The *epoxy resin* group is useful for different material functionalization processes. SU8 UV photosensitive materials are biocompatible, and they are suitable for the preparation of biochemical coupling structures. The epoxy resin group reacts with nucleophile substances (NH<sub>2</sub>) through a special mechanism. It is also possible to perform the transformation of an epoxy group in a hydroxyl group through a hydrolysis chemical reaction that is based on using an acid, basic or capping agent (i.e., ethanolamine). A primary amine reacts with a carboxylic acid or with an epoxide. The basic characteristics of the solution (with a pH of 9) are suitable for this reaction, and the process is followed by deprotonation [73,74].

The side effects of the hydrolysis reaction can be avoided by using an organic solvent such as dimethylformamide (DMF). Regarding the chemical link agents, there are electrophile or nucleophile substances. The electrophile materials accept electrons, and they are epoxy resins, NHS esters, aldehyde R-CHO and carboxylic acid R-COOH, and the nucleophile materials release electrons (primary amine R-NH<sub>2</sub>, thiol R-SH, alcohol R-OH and water H<sub>2</sub>O) [58,59,75,76].

The material morphology could be investigated through infrared spectroscopy, FT-IR transform, X-ray diffraction (XRD), X-ray energy dispersive spectroscopy (EDX), thermogravimetric analysis (TGA), dynamic light scattering (DLS) and zeta potential measurements. The dependence between magnetization and the applied magnetic field is usually measured with a SQUID or vibrating sample (VSM) magnetometers [62]. In Figure 10, different types of analysis made in the case of Fe<sub>3</sub>O<sub>4</sub> nanoparticles are given as examples.



**Figure 10.** Different types of analysis made on  $\text{Fe}_3\text{O}_4$  nanoparticles: (a) X-ray diffraction (XRD); (b) FTIR analysis; (c) DLS investigation; and (d) TGA analysis.

#### 4. Magnetic Properties of MNPs

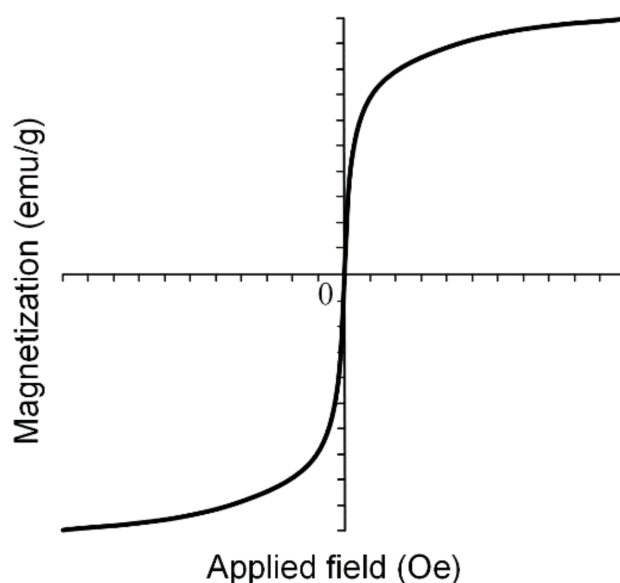
Usually, MNPs are considered to exhibit a ferrimagnetic, ferromagnetic or superparamagnetic behavior. Below a given size of the nanoparticle, which depends on the material type, MNPs are characterized through a zero value of the magnetic moment, in the absence of an external magnetic field, and they are called superparamagnetic particles (SPIONs). The magnetic moment rapidly increases when a magnetic field is acting on MNPs, and it is oriented along the field direction.

SPIONs are very important in medical applications such as magnetic drug targeting, MRI and different cancer treatments due to the fact that when the external magnetic field is removed, SPIONs do not exhibit any magnetic properties and the aggregate formation is prevented. Superparamagnetic nanoparticles present a strong response to external fields, and so they provide a high control of the medical application. In Figure 11, an example of a magnetization curve for iron-based nanoparticles in a superparamagnetic state is shown.

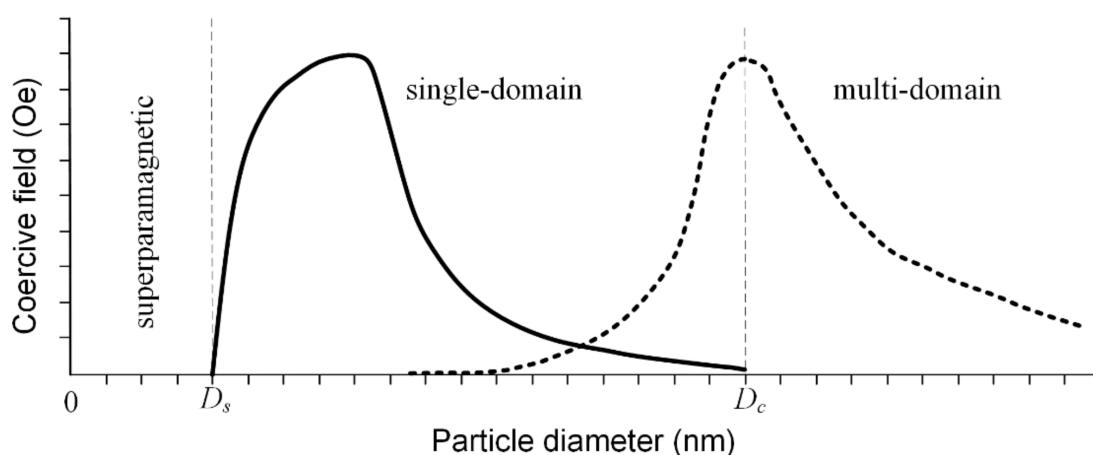
MNPs are characterized through saturation magnetization  $M_s$  (maximum induced magnetization), remanent magnetization  $M_r$  (the value of the magnetization, which can be measured after the magnetic field is removed) and coercivity  $H_c$  (magnetic field strength that is necessary to reduce the magnetization value to zero). In the case of superparamagnetic materials, the dependence  $M(H)$  follows a sigmoidal function, and it presents no hysteresis phenomena [77].

The saturation magnetization is a function of the temperature, and it is well known that above a so-called blocking temperature,  $T_B$  ferrimagnetic and ferromagnetic materials have a superparamagnetic character. This behavior is due to the difference between measuring time and relaxation time as follows: if the relaxation time is lower than the measuring time, the particles are in a superparamagnetic state; otherwise they are in ferrimagnetic or ferromagnetic working conditions [78,79]. When the MNPs' diameter is kept below a

critical value during the synthesis procedure, they are characterized by a single domain structure, and at the lowest diameter value, they are in a superparamagnetic state. If the diameter increases after this critical value, the particle tends to develop a multi-domain magnetic structure (Figure 12). In the case of  $\text{Fe}_3\text{O}_4$  particles, the value of the diameter at which superparamagnetic behavior appears ( $D_s$ ) is around 25 nm, and the critical diameter for the mono-domain magnetic structure ( $D_c$ ) is 82 nm. In the case of  $\gamma\text{-Fe}_2\text{O}_3$ , these values are  $D_s = 30$  nm and  $D_c = 90$  nm [80].



**Figure 11.** Magnetization curve for SPIONs can be modeled using sigmoidal functions. These types of particles do not present hysteresis phenomena, and so after external magnetic field removal, they do not tend to form aggregates.



**Figure 12.** Coercive field variation as a function of the particle diameter, considering the transition between superparamagnetic state to single-domain and to multi-domain state. For the single-domain case, the coercivity variation follows the solid graphical representation in the case of particles that do not interact between them and the dashed line, for the coupled particles.

The size of the MNPs and the synthesis method are directly linked to the saturation magnetization. The value of saturation magnetization  $M_s$  proportionally increases with particle size, and finally it becomes equal to the bulk magnetization value, independent of the synthesis method. Regarding the coercivity field value  $H_c$ , it has a similar behavior, but after a specific size value is reached, a transition from a mono-domain to a multi-domain

structure occurs, and so, as a consequence, a decrease in coercivity is observed [81–83]. In Table 2, the abovementioned magnetic properties in the case of Fe<sub>3</sub>O<sub>4</sub> nanoparticles are summarized.

**Table 2.** Main magnetic properties of Fe<sub>3</sub>O<sub>4</sub> nanoparticles.

Synthesis Method	Size (nm)	$M_s$ (emu/g)	$H_c$ (Oe)	Reference
Aqueous co-precipitation	4.9	60		[81]
	6.3	65		
	8.6	58		
Thermal decomposition	4.2	75	318	[82]
	7.4	70	270	
	8.1	65	70	
	17	82	364	
	45	92	640	
Non-aqueous homogeneous solution of polyols	6.6	71	16	[83]
	11.6	77	15	
	17.8	83	3	

The shape of the magnetic nanoparticles is also an important parameter. Refs. [84,85] analyzed the influence of this parameter, and it was concluded that Fe<sub>3</sub>O<sub>4</sub> spherical nanoparticles have a higher value of  $T_B$  than cubic and spherical Zn<sub>0.4</sub>Fe<sub>2.6</sub>O<sub>4</sub> MNPs, and cubic particles exhibit a higher saturation point when compared with other shapes of nanoparticles.

The magnetic properties of MNPs appear due to the presence or absence of unpaired valence electrons, which are placed on the metal atoms or metal ions. Chemical composition is a very important parameter, and it depends on precursor concentration, synthesis method and dopant nature. The solvent could have an influence on the magnetic state, and so in [78], it was observed that when benzyl alcohol was used, Mn-doped ZnO became paramagnetic and Co-doped MNPs exhibited ferromagnetic properties.

The Curie temperature  $T_c$  of the MNPs, defined as the temperature above which magnetic nanoparticles have a zero value of magnetization, can be varied through chemical composition. This parameter should be carefully controlled, in order to avoid the overheating phenomenon in magnetic hyperthermia. As an example, in the case of aluminum content variation in Y<sub>3</sub>Fe<sub>5-x</sub>Al<sub>x</sub>O<sub>12</sub>, with x between 0 and 2, the  $T_c$  was measured between −40 and 280 °C [78].

## 5. Applications of Magnetic Nanoparticles in Cancer Therapy

The iron oxides with a crystalline core (Fe<sub>3</sub>O<sub>4</sub>) present great potential for use in oncological medicine due to their high compatibility [86], biodegradability [19] and easy synthesis [69]. Additionally, spherical magnetite nanoparticles with a diameter lower than 20 nm exhibit a superparamagnetic behavior that is a very important quality in medical imaging. An iron superparamagnetic particle (SPION) is made from a magnetite magnetic core, which provides the property of contrast in magnetic resonance imaging (MRI). This material has a biocompatible shell with a high number of functional groups, making it very useful for cancerous tumor follow up. Usually, a SPION is a magnetic single-domain structure, and it has high magnetic susceptibility. When such a special nanoparticle is placed in an alternating magnetic field, it can generate heat through Neel and Brown relaxation processes [87]. SPIONs do not have remanence and coercivity, as was explained in Section 4, and their agglomeration in human body is prevented.

Magnetic nanoparticles have received Food and Drug Administration (FDA) approval for the iron treatment deficiency, as a contrast agent in MRI and as a carrier for magnetic drug targeting therapy in different parts of the human body, biotherapeutic transport, magnetic hyperthermy, photothermal ablation, and photodynamic therapy [88].

Magnetic nanoparticles are also used in personalized medicine, termed theranostics. The diagnosis and monitoring of the cancer are performed based on medical imaging

and through chemotherapeutical or biotherapeutical agents such as medicines, nucleic acids and proteins. A clear representation of the tumoral mass is very useful for doctors, because they can anticipate the patient's response when a tumor is surgically removed and the future treatment is established. As medical imaging methods, X-ray radiography, echography, computerized tomography (CT scan), nuclear magnetic resonance (MRI) and positron emission tomography (PET) are analyzed.

The accumulation of magnetic nanoparticles at the tumor sites consists of two types: active or passive targeting. Passive targeting is based on the enhanced permeability and retention (EPR) phenomenon. A characteristics of the tumoral tissue represent the perforated blood vessels, and abnormal lymph drainage can be observed inside the tumor. Nanoparticles with dimensions lower than 100 nm can pass through these broken vessels, and they can migrate inside the tumor and remain there for a longer period of time, as compared with nanoparticle clearance in the blood (EPR phenomenon). Passive targeting is limited, because not all the cancerous tumors in the human body exhibit the EPR phenomenon and the permeability grade of the tumoral vascular system is not homogenous [89,90].

Active targeting is performed through nanoparticle modification, by attaching different groups to the MNP surface. These ligands have the possibility to recognize the biological structure's unicity and neoplasm cells, which accumulate at the tumor site. The magnetic nanoparticles can be guided using an external magnetic field.

It has been proven that the iron oxide nanoparticles can generate microscopic holes inside endothelial cells. This phenomenon is called NanoEL. In order to not block the magnetic nanoparticles in the endothelial tissue, they are delivered through transcellular endocytosis or diffusion transport through the cellular membrane, because junctions between cells appear. The nanoparticles enter into vascularized organs such as the kidneys, liver or spleen at a high speed [91]. The NanoEL effect is much faster in comparison with endocytosis or diffusion through the cellular junction, and it is described in the existence of a intracellular link between the nanoparticle and VE-cadherin [92].

### 5.1. Cancer Cell Monitorization Using SPIONs

Today, the efficacy of the cancer treatment is estimated by taking into account the biopsy tissue analysis or using the medical images of the anatomical structures before and after the treatment. The time between the treatment's initiation and the results' apparition could be weeks or months. With the help of SPION nanoparticles, a real-time monitorization of the treatment is initiated, drugs are delivered, the response of the healthy tissue is evaluated, and the treatment adjustment becomes possible. A successful treatment was obtained in the case of murine dendritic cells with a combination of SPIONs, by increasing the anti-tumorigenic response through T cells stimulation. If dendritic cells are combined with SPIONs, it becomes possible to visualize their trajectories [93].

Other successful studies followed the pharmacokinetics of different active substances using SPIONs in different organs [94–97]. Another application of the SPIONs in drug delivery is made by detecting the changes in the two relaxivity parameters, T1 and T2. The transformation between a non-load state and a load state can be observed. In [98], studies were carried out in which the nanoparticles were used as a carrier for chemotherapeutical medicines, such as doxorubicin combined with Flutax 1 and DiR. The magnetic nanoparticles have a polymeric pH shell that degrades when an acid medium is present. The iron oxide carriers are called "nanophores", and the loading with different active substances increases the SPIONs' transverse T2 and longitudinal T1 nuclear magnetic resonance proton relaxation times. This type of chemotherapeutic treatment has proven to be more effective than classical routes, because the medicines do not have any chemical modification, and they are directly delivered at the tumor site. Drugs such as doxorubicin were modified and combined with polymers and targeting moieties, using the EPR effect. Nutrient receptors such as folate or transferrin receptors were also added to improve the drug delivery. Fluorochrome was used to trace the distribution of molecular groups. Doxorubicin was delivered in liposomal formulations, and clinical studies proved that



higher doses of medicine could be released at the tumor sites, without many significant side effects. Ferumoxytol was approved by the FDA in 2009 to treat iron deficiency. In [98], these MNPs were analyzed as carriers for hydrophobic drugs, which were loaded inside the nanoparticle through the co-incubation process. This innovative delivery system could be approved faster by the FDA, because ferumoxytol is already accepted, and thus developing a way to load the active substances in a clinically approved vehicle will soon be easier in clinical studies. A great advantage of using magnetic nanoparticles consists of the fact that these materials could be followed through MRI and changes in relaxivity parameters.

Ferumoxytol is considered an ideal nanophore in drug delivery, and it was coated with carboxymethyl dextran [99]. After the dialysis process, performed in order to remove accidental cargo substances, the group was loaded with Flutax 1, which is a fluorescent taxol that can link to the taxol microtubule, a site with high affinity. It has been proven that ferumoxytol can also carry a near-infrared fluorophore DiR and the chemotherapeutic active substance doxorubicin. Through the dynamic light scattering method, it was observed that medicine loading has no effect on the average diameter of ferumoxytol, proving that no interactions occur between the nanoparticles and their cargo substances. The prepared colloidal solution has to be stable in a physiological medium (i.e., basic pH), and when the acidic conditions are met, the active substance is released. Ferumoxytol keeps doxorubicin at a pH of 7.2, and then, since pH decreases, it slowly releases the drug [98].

Loading or unloading the iron oxide particles can be observed, without using fluorophores, by analyzing the changes in T2 and T1 parameters and using an MRI device. Slight changes in these parameters were observed at a pH of 6.8. As the pH decreased, rapid decreases were also measured for T2 and T1, suggesting that the active substance is released at the tumor site.

## 5.2. Chemotherapy

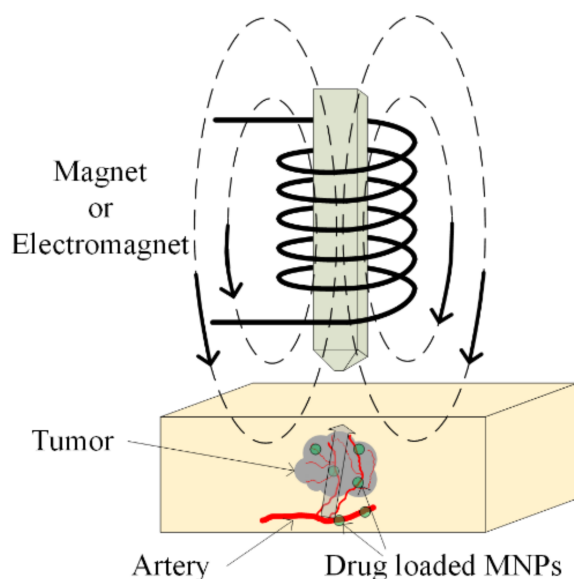
The main aim of chemotherapy treatment is to avoid tumor growth with the help of chemical agents, which inhibit cellular function. The DNA chain can be interrupted by using these agents, and repair of the DNA is prohibited. Sometimes, different types of proteins can be administered to stop the multiplication of damaged cells [100]. The chemotherapeutic drugs do not demonstrate selectivity, and they exhibit a high grade of toxicity in the human body, even acting on healthy cells. To avoid this activity, chemotherapeutic medicines are loaded in magnetic nanoparticles and directly delivered, as was already presented in Section 5.1 at the tumor site (see Figure 13). In this way, the overall toxicity of the treatment is decreased, and the active substance does not demonstrate chemical or physical degradation. In recent studies, TMZ, doxorubicin, paclitaxel and 5-fluorouracil were combined with SPIONs [101–103].

The alkylating agent temozolomide (TMZ) is an imidazotetrazine derivative of dacarbazine and the drug Temodar. TMZ has a lipophilic structure, and it can be orally administered, because the human blood–brain barrier (BBB) is permeable to this substance. The compound presents stability at a pH lower than 5 and at pH higher than 7 if it is hydrolyzed [104].

Temozolomide was approved in 2005 to treat glioblastoma (GBM) patients. Glioblastoma multiforme is grade IV astrocytoma cancer [105]. Firstly, studies were conducted in which a classical treatment approach was taken into consideration. In the first phase of these clinical studies, the patients were administered drugs at doses between 750 and 1000 mg/m<sup>2</sup>, 5 days a week for 4 months. TMZ was combined with radiotherapy and the GBM patients took 75 mg/m<sup>2</sup>/day for 6 weeks, and at the same time focal radiotherapy was applied. Then, they took 150 mg/m<sup>2</sup> TMZ 5 days/week followed by at least 20 days free of cancer treatment [106].

Due to the high toxicity of this drug, poor TMZ penetration across BBB, short half-life, the non-specific nature of the active substance and its non-targeted character, it is better to functionalize it with different ligands (i.e., folic acid) and then load it in

magnetite nanoparticles coated with a polymeric shell, composed of poly(ethylene glycol)-poly(butylene adipate)-poly(ethylene glycol) (TMZ-SPION-PEG-PBA-PEG) [107].



**Figure 13.** Magnetic drug targeting application. Drug-loaded MNPs are directly injected in the arterial blood of the tumor. A magnetic field is applied, and it causes MNPs' enhancement in the tumoral zone.

This shell, formed from three layers of biodegradable and biocompatible polymers, helps to improve the therapeutic efficacy. This hydrophilic shell inhibits the reticuloendothelial system's capacity to recognize and eliminate the MNPs. A higher stability in the physiological fluids observed, and increased blood circulation is obtained. The magnetite hydrophobic core is suitable to be loaded with lipophilic medicines, and their release at the tumor site is controlled.

The magnetic nanoparticles have dimensions between 10 and 100 nm, and thus the accumulation of SPIONs at the tumor zone is performed via the passive targeting process, as well as the EPR effect. Folic acid (FA) can be linked to the folate receptor (FR), which is present in cancerous cells such as GBM, breast and ovarian unhealthy tissues [107].

Another way to prepare an efficient treatment for GBM was proposed in [108], by preparing lipid magnetic nanovectors (LMNVs) loaded with SPIONs and functionalized with transferrin receptor antibodies (anti-TfR Ab). An outer shell made from biotin and m-PEG was analyzed, exploiting a biotin–streptavidin interaction.

Another study described aminosilane-coated SPIONs and took into account the use of magnetic hyperthermia to treat the GBM [109]. If a SPION is loaded with TMZ, its efficacy is increased by using a chlorotoxin (CTX), which has a beneficial effect on the final product's stability [110].

Some studies [111,112], in the case of bladder cancer, have shown that the treatment with mitomycin-C decreased the recurrence rate after 10 years by 40%.

### 5.3. Immunotherapy

The immunotherapy method is an old one, but classical treatments are effective only in a small group of patients. Factors that influence the treatment success are previous treatments, the heterogeneity of the tumor and its stage, and the immunosuppressive phenotype of the cancer [113]. A higher grade of immunogenicity of the tumor ensures a better response to the immunotherapy. This type of therapy increases the immune system response to the cancerous tumor, by stimulating it or by hindering the cancerous cell signal. Artificial antibodies were developed that fight against the tumor, using different routes, such as antigens (Herceptin-targeting HER-2/neu for breast cancer), antibodies, which

sever the blood supply of the tumor, cytokines such as interferon  $\alpha$  and  $\beta$  and immune inhibitors (PD-1 inhibitors) [114,115].

Superparamagnetic nanoparticles are used together with immunotherapy, and the particle dimensions are very important. SPIONs with dimensions lower than 1000 nm are used for liver treatments, and particles smaller than 10 nm can be filtered by the kidneys. Due to lympho-hepatic tropism, SPIONs with intermediate dimensions can form agglomerations in the spine, liver or spleen, and in lymph nodes. These nanoparticles demonstrate an interaction with macrophage monocytes, dendritic cells and tumoral cells, which can be embedded through phagocytosis or micropinocytosis, depending on the surface nature [116,117].

The macrophage cells are phagocytic cells of the innate immune system. They represent the first response of the human body to infections, acting in pathogen recognition, the degradation of cellular intruders, and phagocytosis. Macrophages work well in the presence of T cells, and they induce tissue homeostasis, repair, and reconstruction of the damaged tissue. They also have a great disadvantage, because they are usually associated with autoimmune disease, cancers, angiogenesis, metastasis, and tumor development [118].

Dendritic cells are also a cellular line that detect the existence of pathogens and play an important role in the activation of the immune system. They have antigenic peptides on the major histocompatibility complex (MHC), and induce T-cell activation and differentiation. Dendritic cells are usually called sentinel cells, and they are located inside the lymphoid organs or at interfaces such as the intestines or skin [119].

The human immune system has different mechanisms for transport and integration, in which the magnetic nanoparticles are used in tumor treatment and differential medical imaging. A particular case is lymphatic drainage, realized using magnetic nanoparticles. MNPs are delivered in the lymphatic system, or they are transported by the antigen cells and guided through the lymphatic system to lymph nodes, where MNPs localize in different types of cells, and can regulate the immune system's response. In order to increase the embedding process of the nanoparticles, different types of receptors and antibodies can be linked. Antibodies were used which control the epithelial cells' growth for the encapsulation of the carcinoma cells [120]. If the corresponding cells are not vital for the human body, the antigen differentiation process can be successfully applied.

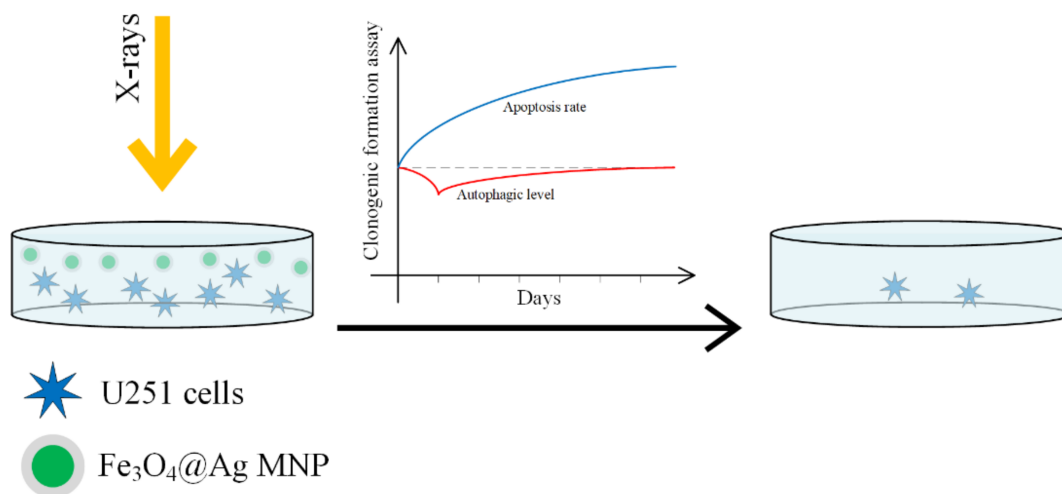
The T anticancer cells are considered indispensable tools for the eradication of different types of neoplasm. If, at the tumor site, an increased number of T cells is detected, the survival rate of the patient increases. T cells have receptors that can recognize pathological cells at the tumor site. By blocking the proteins CTLA-4 and PD-1 through specific antibodies, which are present in drugs, they can restore the entire immune system [121–124]. Pembrolizumab recently received FDA approval for different types of cancers, such as esophageal or gastroesophageal carcinoma, melanoma, applicable for patients with inoperable tumors or metastatic cases, non-small cell lung cancer, small cell lung cancer, head and neck squamous cell cancer, classical Hodgkin Lymphoma, etc. This drug is a monoclonal antibody directed against the PD-1 receptor on the cell surface, and it prevents the binding and activation of PD-L1 and PD-L2 and activates the T cells. Another monoclonal antibody is nivolumab, and it received FDA approval in 2015. Its action route is similar to pembrolizumab, and it can be combined with different chemotherapeutic approaches. It is very suitable for use with MNPs, but the PD-1 monoclonal antibodies target ligands and they can break the link between PD-L1 on cancerous cells and the immune system [125,126]. The first experiments consisted of loading the T cells with SPIONs as vehicles for immune modulatory substances and injecting and guiding them into the tumor sites by applying an external magnetic field [125]. Magnetic nanoparticles have an influence on macrophage polarization modulation, because it is already well known that the macrophage monocytes present two polarization states: non-tumorigenic M1 and pro-tumorigenic M2. In the case of a human monocyte line, it is possible to transform the phenotype M2 into phenotype M1, when SPIONs are used [126–140].

#### 5.4. Radiotherapy

Radiotherapy is one of the most important treatments used to fight cancer. Tumor radiosensitization is an important phenomenon, and it can be enhanced by combining classical radiotherapy with different drugs or even with magnetic nanoparticles. Magnetic nanoparticles present a high value of the atomic number  $Z$  and exhibit important X-ray photon absorption, leading to an increase in secondary electrons that produce human DNA deterioration when the radiation dose is increased [141]. Nanoparticles, which are characterized by a high proton number, are usually linked to increased oxidative stress, expressed by reactive oxygen species (ROS) such as hydroxyl radicals that damages the cells' DNA.

SPIONs were used for a long time as contrast agents in MRI investigations, but they increase the radiosensitivity of the tumor, making the radiotherapy treatments more effective [142–144]. In [145], it was found that the radiosensitizing properties of SPIONs have an influence on the MCF7 breast cancer cells, a fact that was indicated by the production of reactive oxygen species. This effect was analyzed in [146,147] in the case of colon cancer cells, in which SPIONs were combined with a 150 MeV proton beam. When 13 nm iron oxide nanoparticles were concomitantly used with 7.1 keV monochromatic X-rays, the colon tumor cells in murine animal model were drastically reduced [148]. In the radiotherapy treatment domain, energy sources in the MeV range are used, and the Compton effect is present [149].

In [150], the radiosensitizing efficacy of  $\text{Fe}_3\text{O}_4\text{-OA}$ , Ag and  $\text{Fe}_3\text{O}_4\text{@Au}$  nanoparticles was compared on a U251 cellular line (GBM line). A schematic representation of the process is presented in Figure 14.



**Figure 14.**  $\text{Fe}_3\text{O}_4\text{@Ag}$  nanoparticles acting as a nano-radiosensitizer for GBM cellular culture treatment. The MNP radiosensitivity magnification effect is due to a decrease in the autophagy at the beginning of the treatment and followed by an increase in the apoptosis.

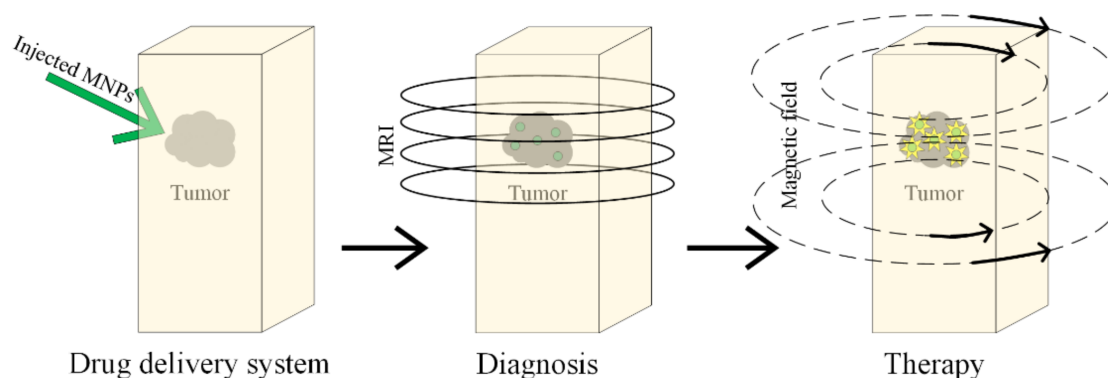
When SPIONs functionalized with gold or silver are used, the surface properties are changed. The gold nanoparticles increase the cellular death rate due to radiation, by interacting with thiols in the cytoplasm. Silver nanoparticles increase radiosensitivity in glioma by inducing cell apoptosis. This enhancement is stronger than in the case of gold nanoparticles [151–155]. SPIONs are guided to the tumor sites with the help of an external magnetic field, they can produce an increase in the local temperature due to magnetic hyperthermia, and through a Fenton reaction they can lead to ROS production. The best results were obtained in the case of  $\text{Fe}_3\text{O}_4\text{@Ag}$ , and it can be concluded that this material has a highly efficient radiosensitivity that adds to the radiation effect and destroys the cancer cell. The classical cell death processes due to radiation are necrosis, apoptosis, and autophagy [156].

Some studies have reported that a combination between growth factor receptor (C225) and  $\text{Fe}_3\text{O}_4@\text{Ag}$  can increase the sensitivity of nasopharyngeal carcinoma cells to radiotherapy, and the radiosensitivity of  $\text{Fe}_3\text{O}_4@\text{Ag}$  is higher than gemcitabine (Gemzar) or 5-fluorouracil [157].

In [158], 38 clinical studies were compared, obtained between 1987 and 2014. This clinical research took into account different types of neoplasm, such as head, neck, esophagus, skin, lungs, etc. Radiotherapy was applied as a singular treatment to 1717 persons, and a combined treatment of radiotherapy and hyperthermia (thermoradiotherapy) was used for 1761 patients. In these cases, an increased rate of survival of 54.9% was recorded, as compared with the rate of 39.8% that was determined for single therapy. The hyperthermic effect of SPIONs increases the radiotherapy's effect [158,159].

### 5.5. Magnetic Hyperthermia

Magnetic hyperthermia has been known about since 1957, and it was first presented in [160], where cancerous tumors were heated with the help of magnetic particles placed in an external magnetic field (Figure 15).



**Figure 15.** Diagnosis and treatment of the tumor based on MNPs, using magnetic hyperthermia.

When magnetic nanoparticles are mediated with magnetic hyperthermia, the treatment is very efficient, because a lot of cancerous cells are killed, and the surrounding healthy tissues are left undamaged [160–165]. This combined treatment is based on intracellular hyperthermia, and it is possible to heat only the harmful cells and the link between cells and targeting ligands with MNPs becomes possible. It can be observed that the local and homogenous heat presents a high grade of selectivity. This type of treatment is in clinical trials for GBM cancer [166].

Magnetic hyperthermia that uses MNPs or SPIONs (SPIONs-MH) is based on locally increasing the temperature above  $42\text{ }^\circ\text{C}$ , with an impact on cancer cell physiology, by altering the structural proteins and generating the necrosis or apoptosis of the cells [162,165,167].

The treatment's success depends on the following factors: (1) the cancerous cells must be selectively targeted; (2) the SPIONs' penetration inside the cancerous cells should be facile; (3) the encapsulation of the SPIONs in the unhealthy cells has to be completed; (4) SPIONs must be biocompatible and non-toxic; (5) the treatment should be feasible from the clinical point of view; (6) the treatment has to be a general one, and different types of tumors can be treated, even metastatic ones [168,169].

The SPIONs-MH have strict limitations regarding the effective value  $H$  and the frequency  $f$  of the alternating applied magnetic field, so the product  $H \times f$  must be strictly lower than  $5 \times 10^9$  due to biomedical conditions [170]. When SPIONs are used, it must be taken into account that sometimes, their low thermal conversion efficiency is due to a decreased value of magnetic susceptibility, and this is an important problem in medical applications. In order to address this limitation and to obtain improved induction heating properties, modulation of the particle size [171], a strict control of the chemical

composition [172–179], biofunctionalization of the SPIONs' surface, and modification of the particle shape [86,180] should be taken into account. It is already well-known that an accumulation of SPIONs in lysosomes, which are known as the “suicidal bags” of the cell, because they can destroy their own cells through specific hydrolytic enzymes, leads to lysosomal cell death by increasing the local temperature and the production of ROS inside the lysosome [181,182].

The heating effect of SPIONs is due to the magnetic hysteresis phenomenon, Neel relaxation, induced eddy currents and Brownian relaxation. The time interval between two random flips of the SPION magnetization due to temperature is known as the Neel relaxation time. SPIONs are ferrimagnetic or ferromagnetic nanoparticles, because they contain iron, and so a small hysteretic dependence between magnetic flux density and magnetic field strength is expected to appear. The energy losses, necessary to magnetize such a material, are usually called hysteresis losses. The heat generated by SPIONs is equal to the hysteresis cycle area, and in the case of a very small nanoparticle, the magnetization of the material is due to spin magnetic moment rotations. When an alternating magnetic field is applied, the spins' rotation must overcome the friction phenomenon, which appears between the easy magnetization axis of the particles and atomic lattices due to the Neel relaxation phenomenon. The friction effect can also be generated between the SPIONs and the area near them in the case of Brownian relaxation. In nano-magnetism, the Neel and Brown relaxation mechanisms are classical processes which completely characterize the single-domain nanoparticle magnetization [77].

If the time necessary to measure the magnetization of the nanoparticle is higher than the Neel relaxation time, in the absence of an external magnetic field, the average magnetization of SPIONs, dispersed in different aqueous solution, is equal to zero [183].

The main experimental technique used for measuring MNPs' magnetic heating is calorimetry, which measures the specific heat absorption rate (SAR), specific loss power (SLP) and intrinsic loss power (ILP) [181,184]. The hysteresis loop of SPIONs or MNPs is determined through alternating current magnetometry. The heat dissipated during a cycle is equal to the hysteresis area, and SAR can be computed as in [171,181], but this type of experimental measurement is performed at different values for the magnetic field strength and frequency that are not in the biological range, and so the magnetic characterization is not entirely accurate for SAR detection [185]. In Table 3, experimental data, obtained in the case of Fe<sub>3</sub>O<sub>4</sub> magnetic nanoparticles with different shape and sizes, are presented [184,185].

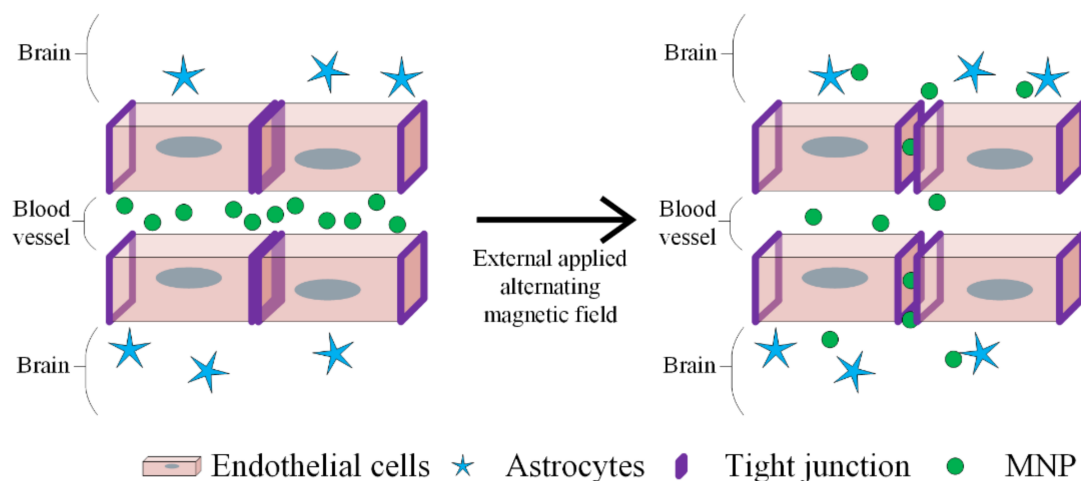
**Table 3.** Shape and size effect on MNPs' magnetic heating parameters for Fe<sub>3</sub>O<sub>4</sub> nanoparticles [184,185].

Shape	Size (nm)	<i>f</i> (kHz)	<i>M<sub>s</sub></i> (emu/g)	<i>H</i> (Oe)	SAR/SLP (W/g)	ILP (nHm <sup>2</sup> /kg)
sphere	22	500	65	195	716	5.96
disc	125	488	435	600	5000	4.48
ring	70	400	-	744	3050	2.18

When the shell of an MNP has been functionalized with a fluorophore through a bond, which can break at a given temperature [186], it is possible to measure the fluorophore content after the heating process, and the bond breaking temperature is determined through fluorescence thermometry.

In the case of the application of an alternating magnetic field, the MNPs develop due to the Joule effect and eddy current losses, which contribute to an increase in the total heating effect. In [187], the thermogenesis of MNPs when an external magnetic field is applied was presented. Films of Au@MNPs present a magnetothermal effect at a high frequency in the order of 10<sup>2</sup> kHz.

MH is a promising therapeutic strategy in GBM treatment, as depicted in Figure 16.



**Figure 16.** BBB disruption using MNPs and applying an alternative magnetic field. The heat generated by MNPs opens up the tight junction to deliver the drugs. The endothelial cells, astrocytes and MNPs are represented by different symbols, as indicated in the figure legend.

SPIONs can be coated with aminosilane, a polymer that improves protein and cell adhesion. This material was used in preclinical investigations [188–190] and in some phase I and II clinical trials [191–196]. The first clinical study was described in [195], and it was applied in the case of 14 GBM patients. The entire group received a 15 nm aminosilane-coated MNP suspension that was neuro-navigationally guided through the tumor site, followed by 4 to 10 thermotherapy applications. At a maximum field value of 14 kA/m in 90% tumor volumes, a temperature between 39 and 46 °C was obtained.

In 2009, a second postmortem study on three GBM patients was developed, and histological analysis showed that MNPs were confined near the tumor sites, demonstrating that it is necessary to administer MNPs in multiple places in order to obtain a uniform heat production [193].

Another clinical study performed on 66 patients using MH in combination with radiotherapy was published in [196]. Although an increased survival rate was obtained, serious side effects such as increased intracranial pressure or necrosis [197] and moderate side effects such as headache, fatigue, thrombocytopenia, leukopenia, vomiting were reported.

The general characteristics of the SPIONs used in MH is that the SAR depends on the particle size, shape, magnetization, chemical composition, and concentration of SPIONs, magnetic field intensity and frequency. It is better that magnetic fields with high oscillation frequencies are avoided due to eddy current generation [198].

Magnetic hyperthermia mediated through SPIONs has proven its efficacy, by causing about 50% cell death of the U87-MG cellular line (GBM—malignant glioma) compared with only 20% cell death in the HUVEC line (healthy endothelial cells) [199]. Zinc-doped ferrite nanoparticles have a higher saturation point than in the case of classical particles and a constant anisotropy energy, and they have proven to be effective for U87-MG by inducing a hyperthermia effect for a frequency of 700 kHz at 1.7 kA/m [200]. The achieved temperature was 41.5 °C, and it was high enough to produce cell death. Human-like collagen protein-coated SPIONs have a rapid heating capacity, by comparing them with uncoated particles, because the MNPs' agglomeration is reduced, and they have an enhanced surface stability [194]. Another approach consists of using iron oxide-coated cationic liposomes, because they present a high cellular affinity and electrostatic interactions with the anionic phospholipids from the cellular membrane. Their effect was investigated on T-9 glioma cells, and a temperature of 42 °C was achieved in 20 min, and as a final result, 100% cellular cancerous death was obtained in 40 min [174,194,199,201,202]. In [194,203], poly-ethylene-glycol-based hydrogel with MNPs, which induces MH, was analyzed on M059K glioblastoma cells, and the results were satisfactory.

Magnetic hyperthermia has a great potential to become a first line treatment for GBM patients and for other cancers. Other studies have incorporated MNPs and methotrexat (MTX) to treat breast cancer [159,204–206]. Other chemotherapeutical medicines, such as doxorubicin, can be combined with MH treatments, making this approach more effective. Another advantage consists of the damage to the extracellular matrix of cancer cells, due to heat effect that facilitates drug elution at the tumor site. These types of studies were performed on a murine animal model.

### 5.6. Gene Therapy

Gene therapy is similar to chemotherapy, and the main difference between them is that instead of delivering small drugs, guided biological agents such as DNA, RNA or siRNA, proteins, and peptides are delivered to the tumor site, and in this way the cellular death can be induced. When cancer appears in one body part, the deteriorated human DNA is characterized through the appearance of atypical proteins, and the disease can be treated through defect gene replacement inside the cancerous cells. Alternatively, siRNA works by suppressing the protein actions, which are due to the cancerous cells. As a classical definition, siRNA is a double-stranded interfering RNA formed from a 21–23-nucleotide sequence. siRNA is combined with nanoparticles that can carry and deliver it to cells, because medical RNA has the property to be very degradable when it is directly injected into the bloodstream [207]. From siRNA, RNA-induced silencing complex (RISC) is produced, which is formed in the cell cytoplasm. The RISC binds the mRNA of the cell. siRNA is usually used to target oncogenes. When siRNA is carried by an MNP, the particle becomes almost unrecognizable for the human body, the cell uptake will be improved, and the circulation time becomes longer. The MNPs will accumulate at the tumor sites and due to tumor vascularization, the particle can easily enter inside the tumor, and the poor lymphatic drainage permits particle accumulation.

The magnetic nanoparticles, which encapsulate or bind DNA or RNA, are covered with a cationic polymer, leading to a positively charged layer, favoring an electrostatic interaction between negatively charged nucleic acid and the MNPs. Other studies showed that for a successful DNA delivery, it is necessary that the MNPs interact with the cell nucleus [208,209]. Recent approaches involved the development of “intelligent” MNPs that use specific coatings, which prevent the delivery carrier from being degraded and permit drug release after entering the tumoral cell. Some initial coatings were performed with disulfide-containing polyethylimine (PEI), and in recent years, polymer shell coatings based on chitosan, PEI, and PEG were developed [210].

In the case of GBM cancer, the tumor presents many genetic aberrations, and cationic-coated MNPs as non-viral vehicles for gene drugs were able to deliver tumor necrosis factor-related apoptosis-inducing ligand (hTRAIL), encoding plasmid open reading frame (pORF-hTRAIL) with high efficiency and survival rate in a rodent glioma model [211]. In the near future, gene delivery with the help of MNPs could become a safe option to treat GBM, because MNPs represent a new way to address infiltrating cells of GBM.

### 5.7. Ferroptosis

Ferroptosis is classified as an oxidative regulated cell death (RCD), and the main involved mechanisms are iron-dependent peroxidation of lipids and plasma membrane rupture [212]. Inside the living cells, the mitochondria represent the most important reactive oxygen species (ROS) source. Ferroptosis can be carried out in two ways: extrinsic or intrinsic. The extrinsic modality consists of cell membrane transporters' (cystine/glutamate) inhibition or by stimulating iron transporters such as serotransferrin and lactotransferrin [213]. The intrinsic pathway is characterized by a blocking of intracellular antioxidant enzymes such as glutathione peroxidase (GPX4). In the case of an increased intracellular amount of lipid reactive oxygen species (L-ROS) that exceed the GPX4, it results in damage to the cellular redox homeostasis [214].



Ferroptosis has three important characteristics, as follows: the oxidation reaction of polyunsaturated fatty acid (PUFA) from the phospholipids of the cellular membrane, the presence of iron as a result of redox chemical reaction, and finally the loss of lipid hydroperoxide's (LOOH) repair properties [215]. It can be concluded that ferroptosis is usually due to a deadly metabolic imbalance, and it can represent an adequate solution for cancers which are resistant to other therapies [216]. Changes that appear in the cell mitochondria, such as volume decrease, bilayer membrane density increase, external mitochondrial membrane disruption, and the absence of mitochondrial cristae [217,218], are important parameters and favor the ferroptosis process. In [219], it was shown that if a clear and spherical cell which contains an empty cytosol is microscopically detected, is considered to be a ferroptotic cell.

From a biochemical point of view, the ferroptotic cell is characterized by the peroxidation of PUFAs in membrane phospholipide due to an increased quantity of redox active divalent iron  $Fe^{2+}$ . This process is controlled through GPX4, which converts LOOH into a lipid alcohol [220].

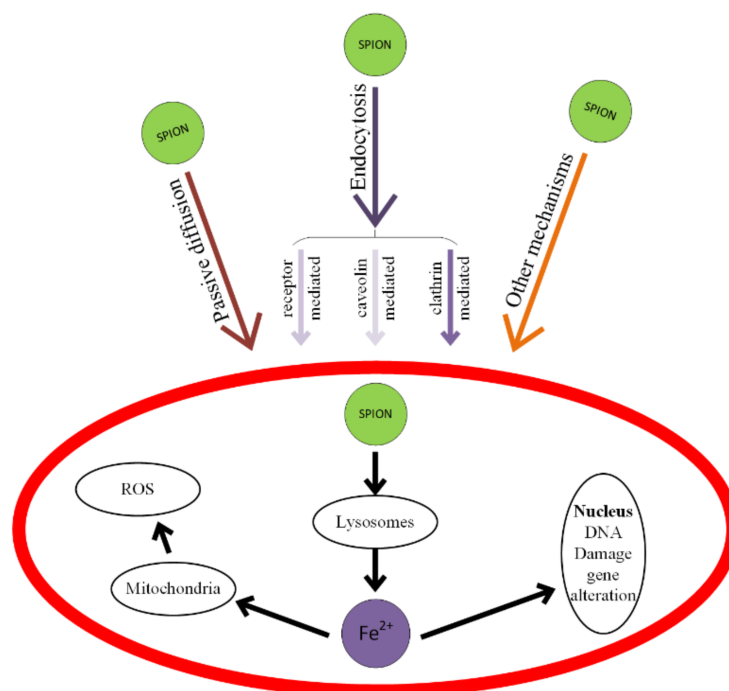
Different genes connected with iron metabolism in the human body (transferrin receptor TFR1, iron response element binding protein 2, IREB2 and ferritin heavy chain FtH), lipid synthesis and oxidative stress pathways are also involved in controlling the ferroptosis process [221,222].

Ferroptosis can be considered an useful tool, because the FDA have approved the so-called ferroptosis inducers (erastin, sorafenib, sulfasalazine (SAS), cisplatin, 1-buthionine sulfoximine (BSO), artesunate (ART), lanperisone, RSL3, altretamine, iron ionophores, doxorubicin into mesoporous carbon nanoparticles/withaferin A/poly(ethylene glycol)-coated (PEGylated) silica nanoparticles, etc.).

SPIONs are very important in this RCD process, because they induce cellular death through an increase in iron level and ROS generation [223]. ROS include superoxide, oxygen peroxide, hydroxyl radical, singular oxygen species, peroxy radical, alkoxy radical, hypochlorous acid, and ozone. In [223], cisplatin with SPIONs as a carrier based on FePt had proven efficacy through the hydrolysis of iron oxide contained in SPIONs. Cancer cells have an acidic pH, which favors iron intracellular release and Fenton-like reaction generation, which produce ROS. The chemical Fenton-like reaction consists of divalent iron  $Fe^{2+}$ 's reaction with hydrogen peroxide ( $H_2O_2$ ), generating ROS [224–226].

When SPIONs, considered as ROS generators through a Fenton-like reaction, are combined with anticancer drugs, the treatment will be more efficient. The toxicity of SPIONs is shown in Figure 17 and consists of cell membrane deterioration, cytoskeleton structural modifications, oxidative damage of DNA chains, lysosome working condition modifications, ROS generation, mitochondria damage, and the generation of inflammatory factors [227,228].

Mitochondria-mediated ferroptosis has a potential use in cancer treatments, but supplementary *in vivo* models to fulfill this theory are necessary at this moment of time [213,221,222,224–227].



**Figure 17.** Mechanisms of SPIONs' interaction with cells and types of induced toxicity. SPIONs mainly interact with cells through passive diffusion or endocytosis. The endocytosis pathways are: clathrin-mediated, caveolin-mediated and other receptor-mediated.

## 6. Challenges and Discussions Regarding the MNPs Use in Cancer Therapy

Nanoparticles are used more and more often in many medical fields as orthopedy, stomatology and neurosurgery. In [229–232], composites consisting of a combination between magnetic nanoparticles, calcium phosphates and biopolymers are prepared through a biomimetic co-precipitation method for bone tissue engineering. In dental restoration, metallic nanoparticles are usually involved in designing adhesives used in coherence tomography evaluation. Graphene-based nanomaterials are another innovative solution for tissue engineering in the dental field [233–235]. Selenium nanoparticles were involved in surface modification of the titanium mesh for cranioplasty [236–238]. In the nanoparticle field, magnetic nanoparticles represent a special class, because they demonstrate an intrinsic association with oncological domain.

Although some MNPs and SPIONs have received FDA approval, their use as treatments in cancer therapy should be carefully conducted and controlled, because a high amount of these materials could be harmful. MNPs and SPIONs can exhibit toxicity, and thus they sometimes are functionalized with different inorganic or organic compounds in order to obtain a passivate surface. Modern vectors for drug-delivery applications are also silica-based mesoporous structured materials, due to their specific textural characteristics, consisting of uniform pores with laboratory-controllable sizes, a high specific surface area and high chemical and thermal stability [60,61]. Different studies, presented in the paper, provide evidence that MNPs have a very low level of toxicity, when their concentration in solutions is lower than 100  $\mu\text{g}/\text{mL}$ . The analysis made *in vivo* or *in vitro* proves that SPIONs can alter living cells due to cytoskeletal deterioration, ROS generation, mitochondria damage, and DNA structure change. It is supposed that the SPIONs' toxicity is not due only to their ferromagnetic or ferrimagnetic cores, but also to nanoparticle agglomerations, which can become instable in biological media or different solutions, similar to body fluids. In the case of SPIONs, the shape (spherical, rod or beam), the dimensions, the outer shell, and the iron/material ratio used for the outer shell (polymer or gold) are important parameters that must be taken into account.

If laboratory-developed magnetic nanoparticles are used in animal models, their toxicity has to be carefully analyzed. A high number of MNPs or SPIONs, FDA-approved or laboratory-developed, were successfully applied on murine animal models. In 2007, clinical studies were initiated regarding the SPIONs used in the treatment of GBM patients, through magnetic hyperthermia. If MNPs are addressed for clinical investigations, the physico-chemical properties, toxicity, and the possibility to become carriers for different drugs have to be considered. The shell of the magnetic core must be biocompatible, and the liver and kidneys have to synthesize them fast. The degraded components must also be smaller than 5 nm.

When SPIONs are used in magnetic hyperthermia, their distribution is uniform and the therapeutical temperature has to be achieved inside the tumor volume, and the surrounding tissue must present minimal damage [228].

MNPs and SPIONs have different side effects, such as liver, brain, skin, stomach function deterioration, with visible symptoms such as hair loss, nausea and vomiting and even nerve damage that could unfortunately be persistent for 10 years [213].

MNPs are monitored with the help of MRI techniques, and this is a very important step in cancer monitorization and drug delivery treatments. Today, MNPs are of great importance, because they are considered very useful in early-stage cancer detection, and in the near future, they may be a viable treatment for patients who suffer from aggressive types of cancer such as GBM. It is expected that this technology will be applied at a medium scale for patients at a global level.

Some studies [213,221,222,224] claim that the side effects of the MNPs used in chemotherapy, radiotherapy, gene therapy, immunotherapy and magnetic hyperthermia can be successfully addressed by the self-defense system of the body.

The most important characteristic of the MNPs is that they can be linked to drugs, antibodies, proteins, enzymes and can directly target a specific organ or tumor site using an external magnetic field. MNPs or SPIONs can be heated in alternating magnetic fields and they can destroy the cancer cells.

An important collaborative work between medical specialists and nanomaterial science researchers is important, because together, they can generate steps forwards to ameliorate or cure cancer. As future perspectives, important progress has been made in the development of new MNPs for pre-clinical cancer theranostics applications. Notable steps were made in the synthesis of efficient magnetite/mesoporous media as drug delivery treatments, and in the near future, complex platform could be developed for cancer treatments [60,61,239]. Few nanomaterials have shown success in clinical cases, because supplementary research must be carried out in order to understand nanomaterial–human cell interactions and biological barriers in different types of cancers [240,241]. There are also industrial barriers because good laboratory practice has to be developed. An increase in the number of preclinical trials with MNPs has been observed, and it is expected that this will evolve into clinical studies, by taking into account the great potential of MNPs to diagnose and treat cancer. The *in vivo* behavior of MNPs must be carefully investigated. In order to obtain a high efficiency of MNP treatments, a size reduction and the use of different bio-compatible shells have to be taken into account. In this way, the blood circulation and the time taken to reach the cancerous tissues is greatly reduced. As we have underlined in the paper, despite MNPs' success in murine models as theranostic agents, their loading capacity and their affinity to target cancer cells must be analyzed and improved if possible. The topic of MNPs is a new and important research domain, which is in continuous development, and synthesis of magnetic drug delivery systems should be investigated. Two very important future perspectives consist of MNPs' elimination from the living body and overcoming the reported long-term toxicity cases.

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